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# Modeling the Static Force of a Festo Pneumatic Muscle Actuator: A New Approach and a Comparison to Existing Models

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**Abstract:** In this paper, a new approach for modeling the static force characteristic of Festo pneumatic muscle actuators (PMAs) will be presented. The model is physically motivated and therefore gives a deeper understanding of the Festo PMA. After introducing the new model, it will be validated through a comparison to a measured force map of a Festo DMSP-10-250 and a DMSP-20-300, respectively. It will be shown that the error between the new model and the measured data is below 4.4% for the DMSP-10-250 and below 2.35% for the DMSP-20-300. In addition, the quality of the presented model will be compared to the quality of existing models by comparing the maximum error. It can be seen that the newly introduced model is closer to the measured force characteristic of a Festo PMA than any existing model.

**Keywords:** pneumatic muscle actuator (PMA); pneumatic artificial muscle (PAM); pneumatic system; pneumatic robot

## 1. Introduction

In recent years, pneumatic muscle actuators (PMAs, Figure 1) were integrated in many robotic systems [1–4] and are still particularly favored, especially in applications that have to be lightweight and powerful.



**Figure 1.** Different Festo pneumatic muscle actuators (PMAs). The depicted connector form is called DMSP. See the data sheet [5] for further information.

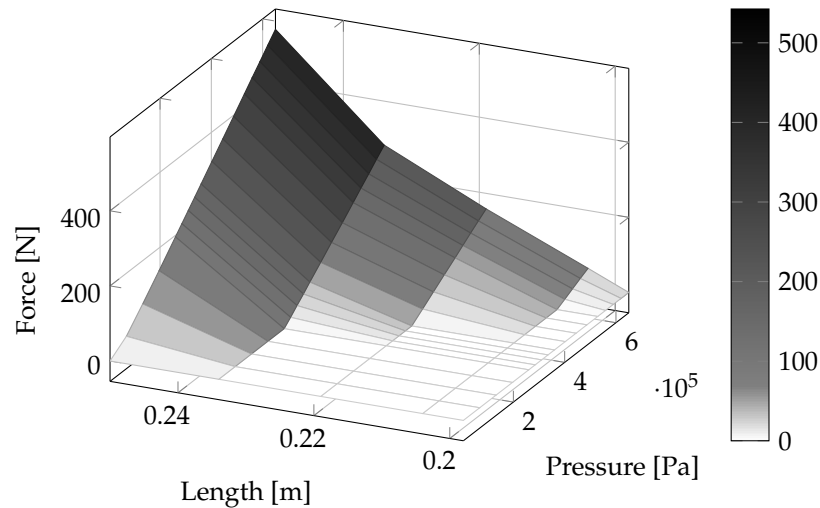
As can be seen in [6], most robotic systems driven by PMAs, but also driven by other actuators, require an underlying torque controller. While integrating PMAs in robotic systems, the control of PMAs and especially the precise torque control of PMA-driven joints consequently becomes an essential feature. The modeling of PMAs, strongly coupled to model-based controller designs, is therefore still a much discussed topic.

On the one hand, PMAs have their own dynamics, like hysteresis [7], some thermodynamic effects [8,9] and can even be interpreted as a spring–damper combination [10]. On the other hand, it has been shown in [11–13] that controlling PMAs, with only a static force map approach, can lead to accurate and high-performance controller designs. The reason is that the PMA dynamics are dominated by the fluid dynamics of the air inside the PMA and the stream of mass characterizing the valve that controls the PMA [14,15]. Nevertheless, a model describing the static PMA force precisely is crucial for the accuracy of the torque controller. Finding the most accurate model to describe the static force characteristic is therefore one goal of this paper.

Different approaches for modeling the static force characteristic of PMAs can be found in literature. The most popular approach is based only on air compression [16]. Although this approach is valid for McKibben PMAs, it is shown by measurements in [14] that this approach does not hold for Festo PMAs. To improve the accuracy of the model presented in [16], the model has been extended in many different ways [8,9,17,18]. It has been shown that these extensions are leading to fewer errors between measured static force maps and the forces predicted by the models. Another approach for the specific use on Festo PMAs has been presented in [12]. The basic idea is the approximation of a Festo PMA as a piston with a virtual, pressure-dependent piston area and a spring that counteracts the expansion. A second approach for the specific use on Festo PMAs is presented in [19], where the static force characteristic is supposed to behave like a mechanical spring with variable stiffness. Because of uncertain parameters, all models, except the first presented in [16], have in common that they must be identified by minimization of the error between a measured static force map and the force defined by the model. By comparing the maximum error, it will be shown in this paper how the accuracy of existing models varies. Furthermore, a new approach for modeling the static force characteristic of Festo PMAs will be presented. The model is physically motivated and therefore gives a deeper understanding of the Festo PMA. After introducing the new model in Section 3 and an explicit discussion of existing models in Section 4.1, all models will be compared to a measured force map of a Festo DMSP-10-250 (DMSP-*initial inner diameter in millimeter*-*initial length in millimeter*) and a DMSP-20-300 in Section 4.3. It will be shown that the error between the new model and the measured data is below 4.4% for the DMSP-10-250 and below 2.35% for the DMSP-20-300. In addition, the quality of the presented model will be compared to the quality of existing models by comparing the maximum error.

## 2. The Static Force Characteristic

A PMA is characterized by its force map. The PMA force  $F_{\text{PMA}}$  is a function of the muscle pressure  $p$  and its length  $L$ , as can be found in [5,17,20,21]. The force map (Figure 2) can be read in the following way: Starting with an unfastened PMA at initial conditions, which means initial length and atmospheric pressure, the PMA does not exert any force. Now putting pressure inside, the PMA gets shorter until it is fully contracted (about 25% [5]). The exerted force is still zero. While pulling the pressurized PMA back to initial length, the PMA will react with the maximum force. The exerted force can be varied between zero and a length-dependent upper limit by varying the PMA pressure [13].



**Figure 2.** Measured static force map of a Festo DMSP-10-250 with an initial length of 250 mm and an initial inner diameter of 10 mm.

### 3. A New Model of the Static Force Characteristic

PMA's are a combination of a flexible tube and two stiff aluminium connectors (see Figure 1). The membrane that the tube is made of is a combination of a stiff aramid fiber mesh and a flexible rubber that encloses the air inside the PMA. While putting pressure inside the PMA, the membrane expands and, due to the stiff aramid fibers, the PMA gets shorter. According to [17], the approach for the presented PMA model also is that the fiber length  $L_{\text{Fiber}}$  stays constant and therefore only the membrane rubber deforms.

#### 3.1. PMA Volume

Following the ideas of [14,15,17], the PMA volume can be approximated by a cylinder. The volume

$$V(L, D) = \frac{\pi}{4} D^2 L \quad (1)$$

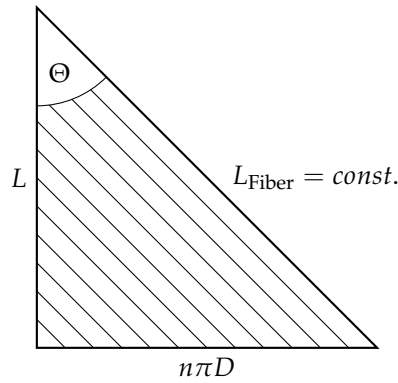
of a cylinder is a function of length  $L$  and diameter  $D$ . Cutting the PMA membrane open and flattening it to a plain (Figure 3), the dependency of the diameter on the length can be calculated by using the Pythagoras theorem [17]. Supposing that  $L_{\text{Fiber}}$  is constant, the diameter equation

$$D(L) = \frac{\sqrt{L_{\text{Fiber}}^2 - L^2}}{n\pi} \quad (2)$$

holds, whereby

$$L_{\text{Fiber}} = \frac{L_0}{\cos \Theta_0} \quad \text{and} \quad n = \frac{L_0 \tan \Theta_0}{\pi D_0}. \quad (3)$$

The index 0 indicates the initial state of the PMA, with atmospheric pressure  $p_0$ , initial length  $L_0$ , inner diameter  $D_0$ , membrane thickness  $H_0$  and fiber angle  $\Theta_0$ . In [14], it is proven by measurements that the initial fiber angle is  $\Theta_0 = 28.6^\circ$ . This is the only value that can be found in literature. The initial membrane thickness,  $H_0 = 1.8$  mm for both the DMSP-10-250 and the DMSP-20-300, can easily be calculated from the given initial inner diameter  $D_0$  and the measurable outer initial diameter of the PMA rubber tube.



**Figure 3.** Unreeled membrane of PMA.

Inserting the functional dependency on the diameter back into the approximated volume (1), the PMA volume loses its dependency on the diameter and is only a function of the PMA length:

$$V(L) = \frac{L \cdot L_{\text{Fiber}}^2}{4\pi n^2} - \frac{L^3}{4\pi n^2}. \quad (4)$$

### 3.2. Energy-Based Modeling

While pulling a contracted PMA, the muscle reacts with a force  $F_{\text{PMA}}$  against the pulling direction. The virtual work of the PMA  $W_{\text{PMA}}$  is given through

$$W_{\text{PMA}} = -F_{\text{PMA}} \cdot dL. \quad (5)$$

Furthermore, the virtual work of the PMA can be separated into two parts. On the one hand, the virtual work  $W_{\text{VAE}}$  has to be done to change the included air volume. On the other hand, additional virtual work  $W_{\text{Elast}}$  is necessary to change the potential energy of the elastic membrane rubber. Therefore,

$$W_{\text{PMA}} = W_{\text{VAE}} + W_{\text{Elast}} \quad (6)$$

always holds.

#### 3.2.1. Virtual Work of the Changing Air Volume

The virtual work needed to change the included air volume inside is given by

$$W_{\text{VAE}} = p \cdot dV. \quad (7)$$

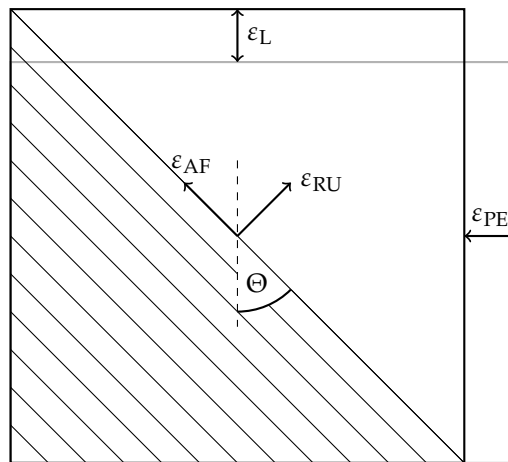
#### 3.2.2. Elastic Energy of the Membrane

While putting pressure inside the PMA, the actuator gets shorter and expands. The deformation of the membrane is a plane state strain and can be described by the strain in direction of the PMA length  $\varepsilon_L$  and the PMA perimeter  $\varepsilon_{\text{PE}}$ . Rotating the coordinate system by the membrane fiber angle  $\Theta$ , the deformation is given by the strain in fiber direction  $\varepsilon_{\text{AF}}$  and the direction of pure rubber  $\varepsilon_{\text{RU}}$  that is perpendicular to the fiber direction (see Figure 4). Following the approach of a constant fiber length, the strain  $\varepsilon_{\text{AF}}$  is always zero. This means that the PMA membrane only expands perpendicularly to the fibers.

For this paper, a one-dimensional state of stress is assumed and, therefore, according to Hooke's law, the tension inside the rubber  $\sigma_{\text{RU}}$  will be approximated by

$$\sigma_{\text{RU}} = E_{\text{RU}}(L) \cdot \varepsilon_{\text{RU}}, \quad (8)$$

where the modulus of elasticity is supposed to be a function of the PMA length.



**Figure 4.** Schematic of the PMA membrane and the fiber angle.

Following the approach of a one-dimensional membrane deformation, the strain

$$\epsilon_{RU} = \sqrt{\left(\frac{L - L_0}{L_0}\right)^2 + \left(\frac{D - D_0}{D_0}\right)^2} \tag{9}$$

is given by the Pythagoras theorem.

Rotating the tension  $\sigma_{RU}$  back to initial coordinates, it is possible to calculate the tension in length direction

$$\sigma_L = \sigma_{RU} \cdot \sin \theta = E_{RU}(L) \cdot \epsilon_{RU} \cdot \sin \theta = E_{RU}(L) \cdot \frac{L - L_0}{L_0} \tag{10}$$

and the tension in perimeter direction of the PMA

$$\sigma_{PE} = \sigma_{RU} \cdot \cos \theta = E_{RU}(L) \cdot \epsilon_{RU} \cdot \cos \theta = E_{RU}(L) \cdot \frac{D - D_0}{D_0}. \tag{11}$$

Multiplying the tension with the edge surfaces of the unreel membrane, the virtual work to deform the membrane in length direction is given through

$$W_{Elast-L} = \underbrace{\sigma_L \cdot H_0 \cdot \pi \cdot D(L)}_{= F_L} \cdot dL. \tag{12}$$

This approach neglects any effect of lateral contraction. The virtual work that is necessary to deform the membrane in perimeter direction can be calculated in an analog way:

$$W_{Elast-PE} = - \underbrace{\sigma_{PE} \cdot H_0 \cdot L \cdot \pi}_{= F_{PE}} \cdot dD. \tag{13}$$

The negative sign in Equation (13) is necessary because an increase in length of the PMA has to result in a decreasing perimeter, and this is defined to be positive for this paper.

### 3.2.3. Summarizing the Energy

Inserting Equations (5), (7), (12) and (13) in Equation (6), the force of the PMA is given by

$$F_{Martens}(p, L) = F_{PMA}(p, L) = -p \cdot \frac{dV}{dL} + F_{PE} \cdot \frac{dD}{dL} - F_L. \tag{14}$$

It must be noted that Equation (14) is positive, in case the PMA exerts a pulling force.

Because the modulus of elasticity of the membrane rubber and the fiber angle cannot be measured directly, both terms are identified by minimization. The modulus of elasticity  $E_{RU}$  used in Equations (10) and (11) is approximated by a polynomial of the third order:

$$E_{RU}(L) = c_3L^3 + c_2L^2 + c_1L + c_0. \quad (15)$$

This order is chosen by experiment. It can be seen that higher order polynomials do not lead to better results. However, for lower order polynomials, the calculated error, defined later in this paper (Equation (23)), is much higher. Furthermore, the approximately known fiber angle  $\Theta_0$  is corrected by a constant  $d_0$ :

$$\Theta_0^{\text{corr}} = \Theta_0 + d_0. \quad (16)$$

$\Theta_0^{\text{corr}}$  is now used as the new, corrected fiber angle. In this paper, all parameters  $c_j$  and  $d_j$  ( $j \in \mathbb{N}_0$ ) have to be identified through solving the minimization problem (22). The parameters  $c_j$  and  $d_j$  are calculated in such a way that the quadratic error between a measured force map and the forces predicted by the models is the smallest. A more detailed discussion of the optimization will be given later in this paper.

#### 4. Validation and Comparison to Existing Models

##### 4.1. Existing Models

Defining a valid model describing the static force characteristic of a PMA is still a much discussed topic. The first model that was introduced to describe a McKibben Muscle [16] was only based on the energy that is needed to change the inner PMA air volume. Effects of elasticity of the membrane material were fully neglected:

$$F_{\text{McKibben}}(p, L) = -p \cdot \frac{dV}{dL} = p \cdot \frac{L_{\text{Fiber}}^2 (3 \cos^2 \Theta - 1)}{4\pi n^2}. \quad (17)$$

It is shown in [14] that the remaining error between the measured static force characteristic of a Festo PMA and (17) is not negligible. The reason for this is that the Festo PMA stores potential energy in its deformed membrane and the McKibben PMA does not.

A modified version of Equation (17) is presented in [8,9], where Equation (17) has been corrected by two additional factors  $c_0$  and  $c_1$ :

$$F_{\text{Andrikopoulos}}(p, L) = p \cdot c_0 \cdot \frac{\pi D_0^2}{4} \left[ \frac{3}{\tan^2 \Theta_0} \left( 1 - c_1 \cdot \frac{L_0 - L}{L_0} \right)^2 - \frac{1}{\sin^2 \Theta_0} \right]. \quad (18)$$

Although the parameters  $c_0$  and  $c_1$  were calculated directly in [8,9], in this paper, both parameters will be identified by solving the minimization (22). A third improved, inspired by Equation (17) model variant is presented in [18]:

$$F_{\text{Sarosi}}(p, L) = (c_0 \cdot p + c_1) e^{\frac{c_2(L_0-L)}{L_0}} + p \cdot \left( d_0 \cdot \frac{L_0 - L}{L_0} + d_1 \right) + d_2. \quad (19)$$

A model for the specific use on a Festo PMA is presented in [12]. This model is a combination of the pressure-virtual-piston-area product  $p \cdot A(L)$  and a length-dependent counter force  $F_c(L)$ . The idea is that the PMA behaves like a combination of a pneumatic piston with a variable piston area and a mechanical spring that counteracts the expansion of the PMA:

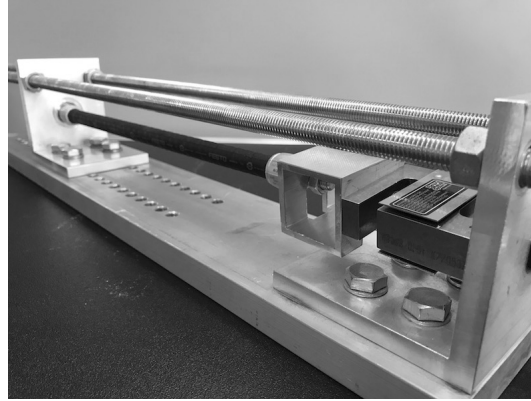
$$F_{\text{Hildebrandt}}(p, L) = p \cdot A(L) - F_c(L) = p \cdot \sum_{j=0}^2 c_j L^j - \left( \sum_{j=0}^3 d_j L^j + d_4 L^{2/3} \right). \quad (20)$$

In [19], the static force characteristic of a Festo PMA is supposed to be equivalent to a mechanical spring, with a displacement-pressure-dependent spring stiffness  $k(p, \Delta L)$ :

$$F_{\text{Wickramatunge}}(p, L) = \underbrace{(c_3 p^2 + c_2 p \Delta L + c_1 \Delta L^2 + c_0)}_{=k(p, \Delta L)} \cdot \Delta L, \text{ with } \Delta L = L - \min(L). \quad (21)$$

#### 4.2. Test Rig

The static force maps of a Festo DMSP-10-250 and a DMSP-20-300 have been measured with the test rig depicted in Figure 5.



**Figure 5.** Photo of the test rig that the characteristic force maps have been measured with.

During the measurement, all screws are fastened and the PMA length is fixed. The pressure is varied between the length-dependent lower limit and the maximum pressure. While varying the pressure, the PMA force is measured by a 1D-forcesensor KD9363-0.5t and a GSV-1A measurement amplifier, both from ME-Meßsysteme GmbH (Hennigsdorf, Germany). Combining the pressure-dependent force characteristics for different lengths, it is easy to determine the static force characteristic as shown in Figure 2. To reduce the influence of measurement errors, the measurement process has been repeated ten times. The depicted force map therefore shows the mean values. Both measured force maps, for the Festo DMSP-10-250 and the DMSP-20-300, can be found in the appendix in Tables A1 and A2, respectively.

#### 4.3. Results

The measured static force maps are characterizing the force behavior of the Festo DMSP-10-250 and DMSP-20-300, respectively. First, the presented PMA models (14), (18)–(21) are identified by minimizing the quadratic error between the measured force map and the force map calculated by the model. The optimization has been solved by using the MATLAB (R2015b, The MathWorks, Inc., Natick, MA, USA) function *fminsearch*:

$$\min \sum_{p_i} \sum_{L_j} (F_{\text{Measurement}}(p_i, L_j) - F_{\text{Model}}(p_i, L_j))^2 \quad (22)$$

$i = \text{Number of pressure points}$   
 $j = \text{Number of length points.}$

Because the optimization problem (22) is nonlinear, only a local, start point-dependent minimum can be found. The start point for all models was identified by iterative testing. It can be seen that good results—in the sense of a small error—can be achieved if the start points are chosen with respect to the physical meaning and within a proper range. According to the SI units—1 m for lengths and  $1 \text{ Pa} = 1 \times 10^{-5} \text{ bar}$  for pressure—any parameter  $c_j$  and  $d_j$  ( $j \in \mathbb{N}_0$ ) is set to 1 if it is only multiplied

to a length-dependent factor and to  $1 \times 10^{-5}$  if it is multiplied by the pressure. The modulus of elasticity of rubber, necessary for Equation (14), is supposed to be in the area of 1 MPa, and therefore the chosen start point is set to  $1 \times 10^6$ . The initial fiber angle  $\Theta_0$  in Equation (14) is supposed to be correct. The chosen parameter estimation's start points for all models are given without units in Table 1.

**Table 1.** Start points of parameter estimation for all models without units.

	$c_0$	$c_1$	$c_2$	$c_3$	$d_0$	$d_1$	$d_2$	$d_3$	$d_4$
$F_{\text{Andrikopoulos}}$	$1 \times 10^{-5}$	$1 \times 10^{-5}$	-	-	-	-	-	-	-
$F_{\text{Wickramatunge}}$	1	1	$1 \times 10^{-5}$	$1 \times 10^{-10}$	-	-	-	-	-
$F_{\text{Hildebrandt}}$	$1 \times 10^{-5}$	$1 \times 10^{-5}$	$1 \times 10^{-5}$	-	1	1	1	1	1
$F_{\text{Sarosi}}$	$1 \times 10^{-5}$	1	1	-	$1 \times 10^{-5}$	$1 \times 10^{-5}$	1	-	-
$F_{\text{Martens}}$	$1 \times 10^6$	$1 \times 10^6$	$1 \times 10^6$	$1 \times 10^6$	0	-	-	-	-

To demonstrate the validity of the the estimated parameters  $c_{0-3}$  and  $d_0$  defining the new model (14), they are given in Table 2. As assumed, the values for the modulus of elasticity are in the range of MPa =  $1 \times 10^6$  Pa, and the initial fiber angle is only slightly corrected by  $-5.73^\circ$  for the DMSP-10-250 and  $-4.18^\circ$  for the DMSP-20-300, respectively.

**Table 2.** Estimated parameters for  $F_{\text{Martens}}$ ; optimization start point is given in Table 1.

	$c_0$	$c_1$	$c_2$	$c_3$	$d_0$
DMSP-10-250	74.085 MPa	-689.20 MPa/m	1.8370 GPa/m <sup>2</sup>	-848.79 MPa/m <sup>3</sup>	$-5.73^\circ$
DMSP-20-300	93.232 MPa	-715.29 MPa/m	1.5483 GPa/m <sup>2</sup>	-502.95 MPa/m <sup>3</sup>	$-4.18^\circ$

All identified models can now be used for calculating their own specific force maps. The error between the calculated and the measured force map

$$err = 100 \cdot \frac{\max(|F_{\text{Measurement}} - F_{\text{Model}}|)}{\max(F_{\text{Measurement}})} \tag{23}$$

is defined as the maximum difference between a measured and a calculated force point, normalized to the maximum measured force. Multiplied by 100, the error is given by percentage and is shown in Table 3.

**Table 3.** Force error of each model by percentage.

<i>err of</i>	$F_{\text{McKibben}}$	$F_{\text{Andrikopoulos}}$	$F_{\text{Wickramatunge}}$	$F_{\text{Hildebrandt}}$	$F_{\text{Sarosi}}$	$F_{\text{Martens}}$
DMSP-10-250	46.1%	20.05%	13.49%	10.12%	5.1%	4.4%
DMSP-20-300	30%	13.04%	8.2%	5.75%	3.59%	2.35%

It can be seen in Table 3 that the presented model is closer to the measured static force map of the Festo DMSP-10-250 and DMSP-20-300 than any existing model. The error of Equation (14) for the Festo DMSP-10-250 is smaller than 4.4% and, for the Festo DMSP-20-300, smaller than 2.35%. Furthermore, it can be seen that Equation (17) leads to a maximum error for both PMAs and does not seem to be accurate enough to describe the static force characteristic of a Festo PMA.

### 5. Conclusions

In this paper, a new approach for modeling the static force characteristic of Festo PMAs is presented. After a detailed derivation of the new model (14), the validity of the model is demonstrated by a comparison to a measured static force map of a Festo DMSP-10-250 and DMSP-20-300, respectively. It is shown that the maximum error between the „true“ force and the one predicted with Equation (14)



is smaller than 4.4% for the Festo DMSP-10-250 and smaller than 2.35% for the Festo DMSP-20-300. Furthermore, it is shown that the presented model is closer to the measured data than any existing model that can be found in literature.

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**Author Contributions:** Mirco Martens was the main author of the manuscript and developed the presented model of a Festo pneumatic muscle actuator. Furthermore, Mirco Martens investigated the new model and all existing models under the aspect of accuracy by comparing them to the measured static force maps. Ivo Boblan was the main supervisor and adviser of the work and contributed to the manuscript by reviewing and revising its contents.

**Conflicts of Interest:** The authors declare no conflict of interest. The founding sponsors had no role in the design of the study; in the collection, analyses, or interpretation of data; in the writing of the manuscript, and in the decision to publish the results.

## Appendix A. Measurement Data

### Appendix A.1. Force Map of DMSP-20-300

**Table A1.** Measured force map of a Festo DMSP-20-300 in [N].

Pressure [Pa]	Length [m]					
	0.296	0.282	0.267	0.25	0.237	0.222
35,000	0	0	0	0	0	0
60,000	54.9	0	0	0	0	0
85,000	113.4	0	0	0	0	0
110,000	179	0	0	0	0	0
135,000	241.8	0	0	0	0	0
146,250	273.3	21.1	0	0	0	0
157,500	300.2	42.9	0	0	0	0
168,750	331	70.3	0	0	0	0
180,000	355.6	93.7	0	0	0	0
197,500	402.5	131	27.7	0	0	0
215,000	446.5	165.2	61.6	0	0	0
232,500	495.9	204.1	92.7	0	0	0
250,000	543.4	244.7	122	0	0	0
281,250	623.5	309.7	170.2	42.8	0	0
312,500	708.8	380.4	221	80.6	0	0
343,750	787.9	443.7	277.4	118.7	0	0
375,000	870.9	518.9	328	157.6	0	0
450,000	1065.2	676.4	462.3	252.1	65.5	0
525,000	1268.9	837.5	587.8	352.3	124.7	0
600,000	1460.1	1004	714.8	443.5	188.1	0
675,000	1653.5	1164.3	840.7	535.8	253.3	0

## Appendix A.2. Force Map of DMSP-10-250

**Table A2.** Measured force map of a Festo DMSP-10-250 in [N].

Pressure [Pa]	Length [m]				
	0.25	0.234	0.219	0.204	0.198
5000	0	0	0	0	0
68,750	32.1667	0	0	0	0
132,500	84.8333	0	0	0	0
196,250	139.5	0	0	0	0
260,000	195.6667	0	0	0	0
285,000	217.6667	17	0	0	0
310,000	239.6667	35.1667	0	0	0
335,000	261.6667	52.6667	0	0	0
360,000	283.8333	71.3333	0	0	0
402,187	321.5	101.5	22.8333	0	0
444,375	359	132.3333	46.1667	0	0
486,562	396.6667	162.5	69.3333	0	0
528,750	434.3333	193.6667	92.1667	0	0
559,062	461.6667	216.3333	109.3333	11.5	0
589,375	488.3333	238.1667	126.3333	23.3333	0
619,688	515.8333	261	142.6667	35	0
650,000	542.5	282.8333	158.6667	46	0

**References**

1. Boblan, I.; Maschuw, J.; Engelhardt, D.; Schulz, A.; Schwenk, H.; Bannasch, R.; Rechenberg, I. A human-like robot hand and arm with fluidic muscles: Modelling of a muscle driven joint with an antagonistic setup. In Proceedings of the 3rd International Symposium on Adaptive Motion in Animals and Machines, Ilmenau, Germany, 25–30 September 2005.
2. Caldwell, D.G.; Tsagarakis, N.G.; Kousidou, S.; Costa, N.; Sarakoglou, I. “Soft” exoskeletons for upper and lower body rehabilitation—Design, control and testing. *Int. J. Humanoid Robot.* **2007**, *4*, 549–573.
3. Balasubramanian, S.; Wei, R.; Perez, M.; Shepard, B.; Koeneman, E.; Koeneman, J.; He, J. RUPERT: An exoskeleton robot for assisting rehabilitation of arm functions. In Proceedings of the 2008 Virtual Rehabilitation, Vancouver, BC, Canada, 25–27 August 2008.
4. Noritsugu, T.; Tanaka, T. Application of rubber artificial muscle manipulator as a rehabilitation robot. *IEEE/ASME Trans. Mechatron.* **1997**, *2*, 259–267.
5. Festo AG. *Datasheet—Fluidic Muscle DMSP/MAS*; Festo AG: Esslingen am Neckar, Germany, 2016.
6. Siciliano, B.; Sciavicco, L.; Villani, L.; Oriolo, G. Motion Control. In *Robotics: Modelling, Planning and Control*; Springer: London, UK, 2009; pp. 303–361.
7. Lin, C.J.; Lin, C.R.; Yu, S.K.; Chen, C.T. Hysteresis modeling and tracking control for a dual pneumatic artificial muscle system using Prandtl-Ishlinskii model. *Mechatronics* **2015**, *28*, 35–45.
8. Andrikopoulos, G.; Nikolakopoulos, G.; Manesis, S. Incorporation of thermal expansion in static force modeling of pneumatic artificial muscles. In Proceedings of the 2015 23rd Mediterranean Conference on Control and Automation (MED), Torremolinos, Spain, 16–19 June 2015; pp. 414–420.
9. Andrikopoulos, G.; Nikolakopoulos, G.; Manesis, S. Novel Considerations on static force modeling of pneumatic muscle actuators. *IEEE/ASME Trans. Mechatron.* **2016**, *21*, 2647–2659.
10. Kerscher, T.; Albiez, J.; Zollner, J.M.; Dillmann, R. Evaluation of the dynamic model of fluidic muscles using quick-release. In Proceedings of the First IEEE/RAS-EMBS International Conference on Biomedical Robotics and Biomechatronics, Pisa, Italy, 20–22 February 2006; pp. 637–642.
11. Hildebrandt, A.; Sawodny, O.; Neumann, R.; Hartmann, A. A cascaded tracking control concept for pneumatic muscle actuators. In Proceedings of the 2003 European Control Conference (ECC), Cambridge, UK, 1–4 September 2003; pp. 2517–2522.
12. Hildebrandt, A.; Sawodny, O.; Neumann, R.; Hartmann, A. Cascaded control concept of a robot with two degrees of freedom driven by four artificial pneumatic muscle actuators. In Proceedings of the 2005 American Control Conference, Portland, OR, USA, 8–10 June 2005.

13. Martens, M.; Passon, A.; Boblan, I. A sensor-less approach of a torque controller for pneumatic muscle actuator driven joints. In Proceedings of the 2017 3rd International Conference on Control, Automation and Robotics (ICCAR), Nagoya, Japan, 22–24 April 2017; pp. 477–482.
14. Boblan, I. Modellbildung und Regelung Eines Fluidischen Muskelpaares. Ph.D. Thesis, Technical University of Berlin, Berlin, Germany, 2010.
15. Tóthová, M.; Pitel, J. Simulation of actuator dynamics based on geometric model of pneumatic artificial muscle. In Proceedings of the 2013 IEEE 11th International Symposium on Intelligent Systems and Informatics (SISY), Subotica, Serbia, 26–28 September 2013; pp. 233–237.
16. Schulte, H. The Characteristics of the McKibben Artificial Muscle. In *The Application of External Power in Prosthetics and Orthotics*; National Academy of Sciences—National Research Council: Washington, DC, USA, 1961.
17. Chou, C.P.; Hannaford, B. Static and dynamic characteristics of McKibben pneumatic artificial muscles. In Proceedings of the 1994 IEEE International Conference on Robotics and Automation, San Diego, CA, USA, 8–13 May 1994; pp. 281–286.
18. Sárosi, J.; Biro, I.; Nemeth, J.; Cveticanin, L. Dynamic modeling of a pneumatic muscle actuator with two-direction motion. *Mech. Mach. Theory* **2015**, *85*, 25–34.
19. Wickramatunge, K.C.; Leephakpreeda, T. Study on mechanical behaviors of pneumatic artificial muscle. *Int. J. Eng. Sci.* **2010**, *48*, 188–198.
20. Kelasidi, E.; Andrikopoulos, G.; Nikolakopoulos, G.; Manesis, S. A survey on pneumatic muscle actuators modeling. In Proceedings of the 2011 IEEE International Symposium on Industrial Electronics, Subotica, Serbia, 8–10 September 2011; pp. 1263–1269.
21. Tsagarakis, N.; Caldwell, D.G. Improved modelling and assessment of pneumatic muscle actuators. In Proceedings of the 2000 ICRA IEEE International Conference on Robotics and Automation, San Francisco, CA, USA, 24–28 April 2000.



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